

Assessment of Insulin Secretion and Insulin Resistance in Human

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The impaired insulin secretion and increased insulin resistance (or decreased insulin sensitivity) play a major role in the pathogenesis of all types of diabetes mellitus (DM). It is very important to assess the pancreatic β -cell function and insulin resistance/sensitivity to determine the type of DM and to plan an optimal management and prevention strategy for DM. So far, various methods and indices have been developed to assess the β -cell function and insulin resistance/sensitivity based on static, dynamic test and calculation of their results. In fact, since the metabolism of glucose and insulin is made through a complex process related with various stimuli in several tissues, it is difficult to fully reflect the real physiology. In order to solve the theoretical and practical difficulties, research on new index is still in progress. Also, it is important to select the appropriate method and index for the purpose of use and clinical situation. This review summarized a variety of traditional methods and indices to evaluate pancreatic β -cell function and insulin resistance/sensitivity and introduced novel indices.

Keywords: Diabetes mellitus; Insulin resistance; Insulin secretion

INTRODUCTION

The prevalence of diabetes mellitus (DM) is increasing among people of all ages worldwide, becoming a major burden on public health care [1]. Insulin, a peptide hormone composed of 51 amino acids is the most important hormone for energy metabolism such as glucose, fat and protein and for maintaining homeostasis. The impaired insulin secretion and action are major contributors to the pathogenesis of DM [2]. Specially, impaired pancreatic β -cell function is a prerequisite for the development of hyperglycemia and DM and progressive loss of β -cell function is associated with worsening hyperglycemia [3,4]. Insulin resistance, initially proposed to describe patients with diabetes requiring high doses of insulin [5], is currently

defined as decreased responsiveness (maximal effect of insulin) or sensitivity (insulin concentration required for a half-maximal response) to metabolic actions of insulin, such as insulin-mediated glucose disposal of muscle and adipose tissue and inhibition of gluconeogenesis in liver [6]. Insulin resistance is also associated with metabolic syndrome, which includes dyslipidemia, hypertension, and obesity, resulting in an increased risk of cardiovascular disease [7]. Assessment of the pancreatic β -cell function and insulin resistance are very important to determine the type of DM and to plan an optimal management and preventive strategy in clinical practice. It is also of value in research fields such as new antidiabetic drug development, many kinds of experimental and clinical study on DM and metabolic disease. A variety of methods and indi-

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ces have been developed to assess the β -cell function and insulin resistance/sensitivity based on static, dynamic test and calculation of their results. However, those remain challenging because of the complexity of the β -cell response to various stimuli, feedback mechanism and insulin signaling and metabolism in organs [8]. In order to solve the theoretical and practical difficulties, research on new index is still in progress. It is also important to understand the theoretical background, advantages, and limitations of each method to choose the appropriate method and index for the purpose of use and clinical situation.

In this review, we summarized a variety of currently applicable methods and indices to evaluate pancreatic β -cell function and insulin resistance/sensitivity and introduced novel indices.

INSULIN SECRETION AND INSULIN ACTION

Insulin is secreted by pancreatic β -cell in response to plasma level of glucose and nutrients (amino acid, free fatty acid) and an additional signal like metabolic factor, neurotransmitter and hormone modulate insulin secretion [9]. Glucose is the major factor controlling β -cell function and survival. Glucose entering β -cell via glucose transporters is rapidly phosphorylated to glucose-6-phosphate by glucokinase and undergoes oxidation in mitochondria, leading to production of adenosine triphosphate (ATP). The rise of ATP/adenosine diphosphate ratio in β -cell leads to subsequent closure of the KATP channel which elicits cell membrane depolarization and allows the entry of Ca^{2+} through the opening of L-type voltage-dependent calcium channels. Raised levels of intracellular Ca^{2+} induce exocytosis of secretory granules containing insulin/proinsulin from pancreatic β -cell. The pharmacologic half-life of insulin is estimated to be between 5 and 8 minutes, and is mainly cleared by insulinase activity within the liver, kidneys, and some other tissues [10].

Glucose induces insulin secretion (GSIS) in a biphasic manner; a rapid, early peak (1st phase) is followed by a second slower and gradually rising peak (2nd phase) [11]. First phase insulin secretion is rapidly stimulated by the increased cytosolic Ca^{2+} and is largely due to the exocytosis of primed (readily releasable) insulin granules. Second phase insulin secretion is slow, activated by cytosolic Ca^{2+} , ATP, and cyclic adenosine monophosphate production, and due to the subsequent supply of new insulin granules for release. GSIS can be modulated by

amino acids, free fatty-acids and non-nutrient secretagogues, such as incretin hormones, growth factors, and neurotransmitters.

Insulin binds to the plasma membrane-bound receptor of the target cell and coordinates the integrative anabolic action of nutrient availability [12]. The insulin receptor (IR), a tyrosine kinase, consists of α and β chains and is also activated by insulin-like growth factor I and II as well as insulin. There are two IR isoforms, A and B, but the B isoform is the primary isoform and more specific for insulin. The B isoform is expressed in liver, muscle, and adipose tissue, thus thought to mediate most metabolic effects of insulin. Binding of these endogenous ligands to the α chain of IR causes structural changes in the β chain by inducing auto-phosphorylation in tyrosine residues. These changes are important for downstream events such as recruitment of the adaptor proteins IR substrates. The downstream of IR activation can be functionally divided into mitogenic and metabolic signals.

The role of insulin in glucose homeostasis is represented by the direct effect of insulin on skeletal muscle, liver and white adipocytes [12]. These tissues require tissue-specific insulin signaling pathways. In skeletal muscle, a representative insulin-acting tissue, insulin promotes glucose utilization and storage by increasing glucose transport and net glycogen synthesis. In the liver, insulin activates glycogen synthesis, increases adipogenic gene expression, and inhibits gluconeogenesis by decreasing gluconeogenic gene expression. In white adipocyte tissue, insulin inhibits lipolysis and increases glucose transport and adipogenesis. Although the effects of insulin vary from tissue to tissue, the proximal components involved in insulin signaling are very similar in all insulin-responsive cells. Moreover, insulin suppresses glucagon secretion from pancreatic α -cells which is itself a potent inducer of hyperglycemia [13].

The 1st phase insulin secretion of GSIS is known to be pivotal in the transition from fasting to feeding through the following functions: inhibition of hepatic glucose production (HGP); inhibition of lipolysis; and preparation of target cells for action of insulin across the endothelial barrier [14]. The 2nd phase insulin secretion of GSIS reduces HGP as in 1st phase, but to a lesser extent [15]. More important, it increases glucose utilization in peripheral tissues [16]. Therefore, although the importance of 2nd phase insulin secretion is relatively underestimated compared to that in the 1st phase, it is important for maintaining glucose homeostasis.

METHODS TO ASSESS PANCREATIC β -CELL FUNCTION/INSULIN RESISTANCE

To fully assess pancreatic β -cell function, both β -cell mass and insulin secretory function should be measured; however, β -cell mass cannot be directly measured in human. In general, β -cell function can be estimated by measuring insulin or C-peptide secreted with insulin from β -cells on an equimolar basis. About half of newly secreted insulin molecules are extracted in the first pass by the liver, and the extent of hepatic insulin clearance depends on the disease state and insulin load [17], in contrast, the C-peptide is not significantly cleared by the liver [18,19]. *In vivo* evaluation of dynamic β -cell insulin release from the hepatic portal vein [20] is rarely practical in humans, so this problem can be addressed by exploiting the properties of insulin and C-peptide that are co-secreted but have different clearance mechanisms [21].

By mathematically modeling (with deconvolution) the time-sequentially measured C-peptide and insulin concentrations under various conditions that stimulate β -cells, the pre-hepatic insulin secretion rate (ISR) can be deduced [22].

By the way, basal β -cell function is measured insulin or C-peptide in static situation but 1st phase, 2nd phase insulin secretion, the dose-response curve between glucose and ISR and maximal insulin secretory function can be measured in dynamic stimulatory condition. For this dynamic test, a single glucose injection (such as single bolus, fixed dose infusion or oral glucose intake), graded glucose infusion (GGI) or hyperglycemic clamp technique were introduced. Furthermore, non-glucose stimulator as glucagon or arginine is used to induce maximal insulin response during dynamic test.

In order to measure whole-body insulin action, specific conditions are required to completely suppress endogenous glucose production and to measure the glucose disposal of each tissue by insulin injected from the outside. Conditions to reach a new euglycemic steady state in the hyperinsulinemic state by infusion of various concentrations of insulin to suppress HGP (which is the main), and continuous glucose infusion to maintain the euglycemic status [23]. At this time, since glucose infusion rate (GIR) reflects the rate of glucose utilization in the body, it is possible to directly measure the systemic action of insulin on glucose utilization. Under these conditions, 80% to 90% of the infused glucose is consumed by skeletal muscle and less than 5% in adipose tissue and negligible in other tissues, so the measured insulin action mostly reflects the insulin sensi-

tivity of skeletal muscle. Therefore, insulin sensitivity can be measured directly by using the hyperinsulinemic euglycemic clamp (HEC) method using these conditions.

Because HEC studies are not feasible in usual clinical condition and studies, measurement of insulin sensitivity by the frequently sampled intravenous glucose tolerance test (FSIVGTT) can be used to assess both hepatic and peripheral insulin resistance and correlates well with the HEC technique [24]. Other surrogate markers of insulin sensitivity are calculated by glucose and insulin values in the fasting state or after an oral glucose tolerance test (OGTT) [25-27]. The homeostatic model assessment (HOMA) from insulin and glucose in the fasting state correlates well with the HEC study [27], but it primarily reflects hepatic insulin sensitivity, since the fasting plasma glucose is determined mainly by the rate of HGP and insulin is the primary regulator of HGP. Therefore, the correlation between HOMA and the HEC is less robust when analyzed in subjects with impaired glucose tolerance [28]. On the other hand, indexes of insulin resistance from the OGTT reflect both hepatic and peripheral insulin resistance [26]. Because significant (30% to 40%) amounts of glucose are taken up by the splanchnic bed during an OGTT and also HGP is less completely suppressed than during the HEC study [29], the plasma glucose concentration during OGTT is affected by both hepatic and peripheral (primarily muscle) insulin resistance. This OGTT-derived indexes correlate well (R; approximately 0.7) with insulin sensitivity measured with the HEC study [26].

Intravenous glucose tolerance test

After an overnight fast, an intravenous bolus of glucose (0.3 g/kg body weight) is infused over 2 minutes starting at time 0. Twenty minutes after glucose infusion, a certain amount of insulin is injected over 5 minutes. In the modified FSIVGTT, exogenous insulin (4 μ U/kg/min) is used [30-32]. Tolbutamide was used instead of insulin in the modified FSIVGTT to stimulate endogenous insulin secretion [32-35]. Blood samples are taken for plasma glucose and insulin measurements at -10, -1, 1, 2, 3, 4, 5, 6, 7, 8, 10, 12, 14, 16, 20, 22, 23, 24, 25, 27, 30, 40, 50, 60, 70, 80, 90, 100, 120, 160, and 180 minutes. Two phases of insulin release are observed during FSIVGTT. FSIVGTT can represent β -cell response to rising glucose level in the condition similar to eating. In FSIVGTT, glucose is intravenously injected and stimulate directly the β -cells. Because it does not have to pass through the digestive system, it is free from incretin effect and various gastric emptying time compared with

OGTT. FSIVGTT is influenced by insulin and glucose clearance.

Minimal model analysis was developed by Bergman et al. [36]. Data obtained from FSIVGTT are calculated using the computer program MINMOD to generate an index of β -cell function, insulin sensitivity and glucose effectiveness. C-peptide can be used instead of insulin in minimal model analysis with FSIVGTT.

Minimal model analysis is defined by two couple differential equations, describing glucose dynamics in a mono-compartmental “glucose space” and insulin dynamics in a “remote compartment.” Minimal model uniquely identifies model parameters that determine a best fit to glucose disappearance during the modified FSIVGTT. Minimal model analysis is less labor-intensive than hyperglycemic clamp and does not require steady-state conditions, and does constant intravenous infusion rate control. But, minimal model analysis excessively simplifies the normal physiology of glucose metabolism, resulting in poor accuracy [37,38].

Hyperglycemic clamp test

In hyperglycemic clamp, a high target glucose concentration, which is enough to stimulate insulin secretion, would be maintained by infusion of glucose. A pre-determined priming dose of dextrose is infused for 15 minutes to raise the glucose concentration to a hyperglycemic target level in a short time, followed by an infusion of 20% dextrose for 120 minutes at variable rates to maintain plasma glucose levels at a constant level. Blood samples for plasma glucose and insulin are collected at baseline, every 2 minutes during the first 15 minutes, and then, every 5 to 10 minutes for glucose and insulin measurement during the test. Acute insulin response (AIR) during the first 10 minutes, late insulin response between 10 and 120 minutes are measured [39]. In the presence of hyperglycemia, glucagon (1 mg) can be administered intravenously at 120 minutes to induce an insulin response to non-glucose stimulation. After glucagon injection, additional blood samples are collected at 1, 3, 6, and 10 minutes [40]. The Arginine stimulation test can be performed to evaluate maximal β -cell function at the end of hyperglycemic clamp test [41]. After achieving a plasma glucose concentration up to 350 mg/dL by glucose infusion, baseline samples were taken at ± 5 and ± 2 minutes. A maximally stimulating dose of arginine hydrochloride (5 g) was then injected intravenously for 45 seconds. Samples were taken at 2, 3, 4, and 5 minutes after injection. Hyperglycemic clamp is a

highly reproducible and reliable assessment of β -cell responsiveness to glucose. However, this method has technical difficulty, and it is expensive and is time- and labor-intensive.

Hyperinsulinemic euglycemic clamp test

The HEC test, developed by DeFronzo et al. [39], is widely accepted as the gold standard for the direct determination of insulin resistance/sensitivity in humans [42]. Insulin is administered intravenously at a constant rate (5 to 120 $\mu\text{IU}/\text{m}^2/\text{min}$) after an overnight fast. The new equilibrium insulin concentration is maintained at a higher concentration than in the fasting state. At this time, HGP is suppressed and glucose uptake in muscle and adipose tissue is increasing. In this state, blood glucose levels are frequently monitored at intervals of 5 to 10 minutes with a glucose analyzer, while 20% dextrose is administered intravenously to maintain a blood glucose level in the normal range (euglycemic). An infusion of potassium phosphate is also given to prevent hypokalemia resulting from hyperinsulinemia and increased glucose disposal. After several hours of insulin infusion at a constant rate, an equilibrium state is reached in which plasma insulin, blood glucose, and GIR are kept constant. “Steady-state” is defined as a period greater than 30-minute (at least 1 hour after initiation of insulin infusion) during which the coefficient of variation for blood glucose, plasma insulin, and GIR is less than 5% [6,43]. Assuming that hyperinsulinemia sufficiently inhibited HGP, the GIR is consistent with the glucose disposal rate (M) since there is no difference between the infused and utilized glucose under this equilibrium condition (Fig. 1) [43]. M is corrected for body weight, especially fat-free mass. Thus, the HEC can measure whole body glucose disposal (mainly in skeletal muscle) directly at a given level of hyperinsulinemia under steady-state. When radiolabeled glucose tracers are used under clamp conditions, it is possible to simultaneously quantify HGP as well as whole body glucose disposal [44,45]. When insulin sensitivity is increased, the administered glucose amount is increased. In this case, the difference in blood glucose level between the arterial and venous blood is also increased. Therefore, if the GIR is determined based on the concentration of glucose measured in venous blood, insulin sensitivity may be over-measured. To solve this problem, the hand used for blood sampling may be cannulated in a retrograde fashion and warmed with a heating pad (opening arteriovenous anastomoses) to “arterialize” the venous blood [46]. Radiolabeled tracers of glycerol or amino acids may be used during the HEC to assess insulin sensitivity

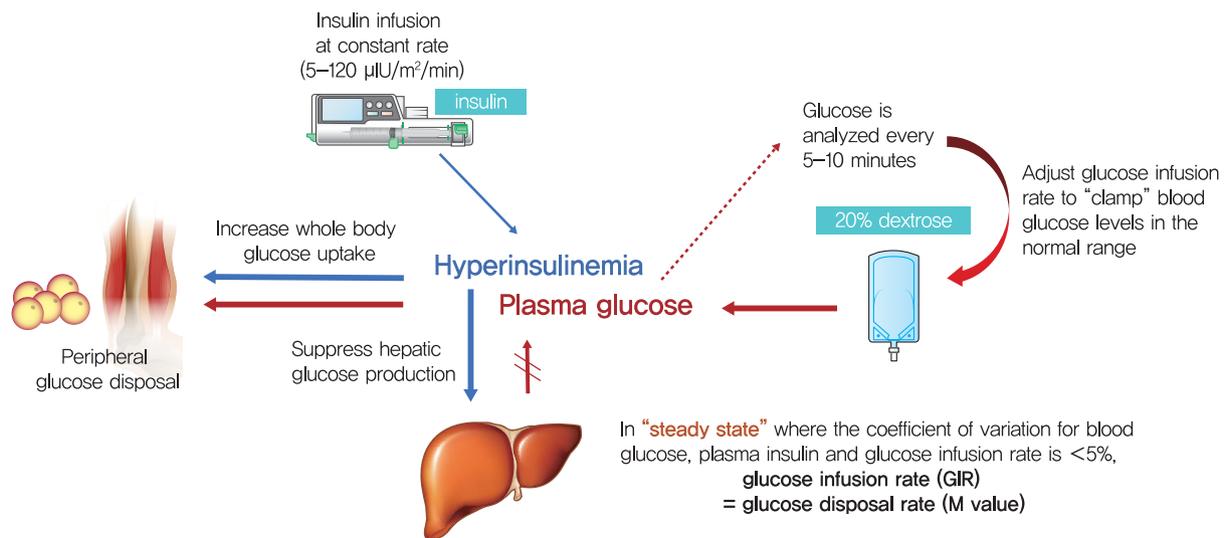


Fig. 1. Hyperinsulinemic-euglycemic glucose clamp technique.

with respect to lipolysis or protein metabolism [47,48]. ^{31}P magnetic resonance spectroscopy may be used in conjunction with the HEC to assess rates of insulin-stimulated muscle mitochondrial ATP synthase flux and insulin-stimulated increases in concentrations of intramyocellular inorganic phosphate [49]. Doppler and contrast ultrasound imaging have also been used in conjunction with the HEC to study insulin sensitivity concerning vascular actions of insulin [50]. However, HEC study takes a lot of time and is a labor intensive and expensive. In addition, it is not suitable for use in large-scale epidemiologic studies and routine patient care because it requires a skilled operator. The HEC may not accurately reflect insulin action and glucose dynamics under physiological conditions that a dynamic test such as an oral meal or oral glucose load may determine.

C-peptide minimal models with graded glucose infusion

After an overnight fast, catheters are placed into both forearm for blood sample collection and glucose infusion. Glucose is administered at progressively increasing and then decreasing rates (0, 4, 8, 16, 8, 4, 0 mg/kg/min). Each glucose infusion is administered for 40 minutes. Glucose and c-peptide levels are measured at 10-minute intervals during a 40-minute baseline period before the glucose infusion and throughout the 240-minute glucose infusion. Both basal and dynamic insulin secretory responses and β -cell sensitivity can be calculated using the C-peptide minimal models [51]. The ISR can be assessed using minimal model analysis computer software [52].

Because it is simpler than minimal model analysis with FSIVGTT, it can widely applied to clinical studies but the incretin effect is not reflected.

Oral glucose tolerance test

OGTT is the most widely used test in clinical practice to diagnose glucose intolerance and DM [53]. After overnight fast, blood samples for determinations of glucose and insulin concentrations are taken at 0, 30, 60, 90, and 120 minutes following a standard oral glucose load (75 g). β -cell function estimated from OGTT presents a more physiological pattern of the changes in glucose, insulin, and incretin hormones than the hyperglycemic clamp or FSIVGTT [21,54]. OGTT is easy to perform but cannot clearly reflect and distinguish the 1st and 2nd phases insulin secretion due to the variability in the glucose concentration.

Mixed meal tolerance test

Mixed meal tests were developed to reflect insulin and glucose responses to the various nutrients along with glucose. There are many kinds of mixed meal with various nutrient distribution composition (for example, 10 kcal/kg, 45% carbohydrate, 15% protein, and 40% fat). Blood samples were collected for glucose, insulin, and C-peptide concentration in fasting state and at 15, 30, 60, 90, 120, 180, and 240 minutes after mixed meal ingestion [53,55]. Like OGTT, the mixed meal tolerance test (MTT) mimics the glucose and insulin dynamics of physiological conditions more closely than the conditions of the hyper-

glycemic clamp, insulin suppression test (IST), or FSIVGTT. But, because of variation of glucose absorption and splanchnic glucose uptake, mixed MTT has poor reproducibility.

Insulin suppression test

The IST is used to directly measure insulin resistance. It was developed by Shen et al. [56] and modified by Harano et al. [57]. After an overnight fast, somatostatin (250 µg/hr) or the somatostatin analog octreotide (25 µg bolus, followed by 0.5 µg/min) is intravenously infused to suppress endogenous secretion of insulin and glucagon. It is assumed that the somatostatin infusion is sufficient to completely suppress endogenous insulin and glucagon secretion. A constant dose of insulin (25 µIU/m² · min) and glucose (240 mg/m² · min) is then infused into the same antecubital vein for 3 hours. From the contralateral arm, blood samples for glucose and insulin are collected every 30 minutes for 2.5 hours and then at 10-minute intervals from 150 to 180 minutes of the IST. Steady-state conditions are more easily achieved with the IST than with the HEC because of the lack of variable infusions. In individuals with marked insulin sensitivity, hypoglycemia may occur during the IST, and in individuals with type 2 DM, glucosuria may occur due to hyperglycemia, making it difficult to accurately measure insulin resistance. Somatostatin infusion can independently affect peripheral glucose clearance [58]. Therefore, IST is limited application in a large-scale epidemiologic studies or clinical trials.

Glucagon stimulation test

Glucagon stimulation test (GST) was described in 1977 [59]. Baseline serum C-peptide and plasma glucose sample are collected. An 1 mg glucagon is injected over 10 seconds. Samples are collected at 2, 4, and 6 minutes after glucagon administration. GST is a more sensitive and reproducible test compared to provocation test using other substrates, such as glucose or tolbutamide. And it is associated with diabetes type and future use of insulin. The majority of patients experienced nausea with the GST.

INDICES OF PANCREATIC β-CELL FUNCTION

First- and second-phase insulin secretion

During FSIVGTT, the 1st phase insulin secretion or AIR is represented as insulin release during the first 10 minutes after

glucose injection [60], and calculated using the area under the curve (AUC) of insulin concentration during the first 10 minutes or mean of the 3, 4, and 5 minutes insulin values after glucose injection minus the basal value. Insulin secretion peaks in 3 to 10 minutes, at which time 40 µIU/mL or less is a low response, and more than 140 µIU/mL is a high response. The 2nd phase insulin secretion is calculated as the insulin area above the pre-stimulus level during 10 to 60 minutes after glucose bolus [61].

In minimal model analysis with FSIVGTT, first phase β-cell responsivity (Φ_1) is calculated amount of insulin released during the first peak in proportion to change in the glucose level. second phase β-cell responsivity (Φ_2) is calculated as amount of insulin released during the second phase.

During hyperglycemic clamp, AIR is AUC of insulin concentration during the first 10 minutes. And late insulin response is AUC of insulin concentration between 10 and 120 minutes. The acute insulin response to arginine (AIRarg) was calculated as the mean of the 2, 3, 4, and 5 minutes values minus the mean of the baseline values [41]. The AIRarg during the 230 mg/dL of glucose clamp allows for determination of the glucose-potential of arginine-induced insulin release (AIRpot). The AIRarg during the 340 mg/dL of glucose clamp allows for determination of the maximal potentiation of arginine-induced insulin release (AIRmax) since the acute responses to arginine are maximal at plasma glucose concentrations 315 mg/dL.

C-peptide

Because the half-life of C-peptide is longer (20 to 30 minutes) than that of insulin (3 to 5 minutes), and hepatic clearance of C-peptide is negligible, and clearance rate in the peripheral circulation is constant compared with insulin [62]. In healthy subjects, the plasma concentration of C-peptide in the fasting state is 0.3 to 0.6 nmol/L, with a postprandial increase to 1 to 3 nmol/L [63]. Spot or 24 hours urinary C-peptide, urinary C-peptide to creatinine ratio can be performed. C-peptide represents endogenous insulin production, and measurement of C-peptide does not have the pitfall of cross-reaction of assay between exogenous and endogenous insulin in insulin-treated patients with diabetes. C-peptide also correlates with type of disease, duration of diabetes, as well as age of diagnosis. Because the majority of C-peptide is metabolized by the kidneys and then excreted in urine [64], C-peptide measurement is inaccurate in patients with chronic kidney disease. And C-pep-

tide metabolism is influenced by age, sex, obesity, body shape, and degree of glucose tolerance [65]. The detection of subtle levels of C-peptide limited.

In addition, fasting or postprandial C-peptide to glucose ratio (CPRI) was suggested as a practical marker of β -cell function in diabetes, especially, postprandial CPRI in type 2 DM [66]. C-peptide concentrations were markedly different and higher in the up and down GGI compared with FSIVGTT, it represents an effect of the glucose perturbation or static and dynamic glucose control. β -Cells are more sensitive to a slow glucose increase, but β -cells response to a decreasing glucose stimulus.

Insulinogenic index

The insulinogenic index (IGI) is used to quantify the β -cell response according to the change of plasma glucose level. IGI is calculated from change in insulin/change in glucose over the first 30 minutes after the load on OGTT.

$$\text{IGI} = \frac{[\Delta\text{insulin (30-0 minutes)} (\mu\text{IU/mL}) / \Delta\text{glucose (30-0 minutes)} (\text{mg/dL})]}{}$$

IGI is also calculated from a mixed MTT. β -Cell function parameters were higher during a mixed MTT than during an OGTT, it suggests that β -cell function parameters are influenced by meal composition [67].

Homeostatic model assessment of β -cell function

HOMA was developed in 1985 as a model for the correlation between glucose and insulin dynamics [27]. Both the original HOMA and the updated HOMA2 assume a feedback loop between the liver and β -cell. For example, glucose concentration is regulated by HGP via insulin, and insulin concentration is regulated by the response of pancreatic β -cells to glucose concentration. It can be used as an index representing insulin resistance and β -cell function. Homeostatic model assessment of β -cell function (HOMA- β) is a simple static assessment of β -cell function using basal values of glucose and insulin [27].

$$\text{HOMA-}\beta = \frac{[\text{fasting plasma insulin } (\mu\text{IU/mL}) \times 360 / (\text{fasting plasma glucose (mg/dL)} - 63)]}{}$$

Because HOMA- β is easy and simple, it is widely used in epidemiologic studies. HOMA- β has a limitation because fasting level of glucose and insulin at a single time point cannot represent the complex relationship between variables in glucose-insulin feedback system. And accurate insulin assay is required for reliable HOMA- β value [42].

Disposition index

Disposition index (DI) is expressed by calculating the product of insulin secretory capacity and insulin sensitivity. Alternatively, it is calculated by dividing the insulin secretory capacity by the insulin resistance value [68]. DI is the concept of insulin secretion capacity taking into account insulin resistance. In healthy subjects, the product of insulin sensitivity and insulin secretion is constant. Insulin secretion increases to response to increasing the insulin resistance, but when β -cell failure occurs, the capacity to compensate for insulin resistance decreases, resulting in lower DI. Thus, DI does not simply indicate insulin secretion but is considered to be a more useful and practical indicator of β -cell function by indicating the insulin secretory ability reflecting the insulin resistance state of each subject.

The index for measuring β -cell function described so far is summarized in Table 1. According to the measurement method, it is classified into a dynamic test and a static test, and the calculation formulas for various insulin secretion indices calculated based on the values of insulin, C-peptide, and glucose measured through each test are summarized. In order to evaluate acute and late insulin secretory function and maximum insulin secretory capacity, dynamic test-based measurement is required. An appropriate method should be selected and utilized according to the strengths and weaknesses of the indices, the environment where they can be used, and the purpose.

INDICES OF INSULIN INSENSITIVITY/RESISTANCE

Insulin sensitivity index

Insulin sensitivity index (SI) is calculated from HEC.

$$\text{SI}_{\text{Clamp}} = M / (G \times \Delta I) [25]$$

M: glucose disposal rate,

G: steady state blood glucose concentration,

ΔI : difference between fasting and steady-state plasma insulin (SSPI) concentrations

For accurate measurement for M and SI_{Clamp} in HEC test, it is important that the assumption that HGP is completely suppressed by steady-state hyperinsulinemia is met [25,45,69,70].

Steady-state plasma glucose concentrations

During IST, the period from 150 to 180 minutes is regarded as the steady-state period, and at this time, the constant infusions of insulin and glucose will determine the SSPI and steady-state plasma glucose (SSPG) concentrations. SSPI concentrations

Table 1. Indices of pancreatic β -cell insulin secretory function

Method	Measurement of β -cell function
Dynamic test-based	
FSIVGTT	First-phase insulin release or AIR: AUC of insulin concentration during the first 10 min of glucose injection or mean of 3, 4, and 5 min insulin values after glucose injection Second-phase insulin release: the insulin area above the prestimulus level during 10–60 min after glucose pulse DI: AIR adjusted for insulin sensitivity (M value)
Hyperglycemic clamp	AIR: AUC of insulin concentration during the first 10 min Late insulin response: AUC of insulin concentration between 10–120 min AIR _{max} : AIR with arginine stimulation.
Minimal model analysis with FSIVGTT	Computational model Φ_1 : first phase β -cell responsiveness which is calculated as amount of insulin released during the first peak in proportion to change in the glucose level Φ_2 : second phase β -cell responsiveness which is calculated as amount of insulin released during the second phase
C-peptide minimal models with graded glucose infusion	Computational model $SR(t) = SR_s(t) + SR_d(t)$
OGTT or MTT	Calculated from OGTT or mixed MTT $IGI = [\Delta\text{insulin (30–0 min)} (\mu\text{IU/mL}) / \Delta\text{glucose (30–0 min)} (\text{mg/dL})]$ Calculated from OGTT or mixed MTT Oral DI: $IGI / \text{HOMA-IR}$ or $[AUC_{\text{insulin}} / AUC_{\text{glucose}}] \times \text{Matsuda index}$
Static test-based indices	
Simple surrogate markers	
HOMA method	$\text{HOMA-}\beta = [\text{fasting plasma insulin } (\mu\text{IU/mL}) \times 360 / (\text{fasting plasma glucose (mg/dL)} - 63)]$
Fasting C-peptide	Fasting C-peptide measurement
C-peptide to glucose ratio (CPRI)	$\text{C-peptide (ng/mL)} / \text{glucose (mg/dL)} (\times 100)$

FSIVGTT, frequently sampled intravenous glucose tolerance test; AIR, acute insulin response; AUC, area under the curve; DI, disposition index; SR_s , secretion rate by glucose concentration (static glucose control); SR_d , secretion rate by the rate of change of glucose concentration (dynamic glucose control); OGTT, oral glucose tolerance test; MTT, meal tolerance test; IGI, insulinogenic index; HOMA-IR, homeostatic model assessment of insulin resistance; HOMA- β , homeostatic model assessment of β -cell function.

are generally similar among subjects, while the SSPG concentrations are inversely related to insulin sensitivity. Thus, SSPG concentration will be higher in insulin-resistant subjects and lower in insulin-sensitive subjects, which can be used as an indicator of insulin resistance/sensitivity. The SSPG is a highly reproducible direct measurement of metabolic actions of insulin, which is less labor-intensive and less technically demanding than the HEC.

Insulin sensitivity (S_i) and glucose effectiveness (S_G)

Insulin sensitivity (S_i) and glucose effectiveness (S_G) is calculated from minimal model analysis. S_i is defined as fractional glucose disappearance per insulin concentration unit. S_G is defined as the ability of glucose *per se* to promote its own disposal and inhibit HGP in the absence of an incremental insulin effect [68,71,72].

1/Fasting insulin

1/Fasting insulin is well known as a surrogate indicator of insulin resistance, which decreases as an individual's insulin resistance increases [73]. However, because insulin concentrations are not normally distributed, linear correlation between $1/(\text{fasting insulin})$ and insulin resistance from HEC method are not strong. And insulin secretion is decreased in hyperglycemic condition in diabetic subjects or glucose-intolerant subjects, which may cause erroneous results. Thus, $1/(\text{fasting insulin})$ had limited use in patients with glucose intolerance or diabetes. There is a lack of standardized insulin assays.

Glucose/insulin ratio

The fasting glucose/insulin ratio (G/I ratio) was used as an index of insulin resistance/sensitivity in previous studies [74–76]. However, the G/I ratio does not appropriately reflect the physi-

ology underlying the determinants of insulin sensitivity [77]. In healthy subjects, fasting G/I ratio is functionally equivalent to $1/(\text{fasting glucose})$ due to fasting glucose levels in the normal range. But, in condition of relative fasting hyperinsulinemia in patients with glucose intolerance or diabetes, fasting G/I ratio erroneously increases compared to $1/(\text{fasting glucose})$. In patients with diabetes, the fasting insulin concentration is low and the maintaining blood glucose in the normal range is insufficient; thus, there are limitations in applying these surrogate indices derived to patients with diabetes.

Homeostatic model assessment of insulin resistance

$$\text{HOMA-IR} = [\text{fasting insulin } (\mu\text{IU/mL})] \times [\text{fasting glucose } (\text{mmol/L})] / 22.5$$

Homeostasis model of insulin resistance (HOMA-IR) is simple, minimally invasive, but insulin resistance in patients treated with insulin needs further validation. The denominator of 22.5 is a normalizing factor. HOMA-IR has a reasonable linear correlation with HEC and minimal model estimates of insulin resistance in several studies of distinct populations [78, 79]. Log (HOMA-IR) represent a much stronger linear correlation with HEC estimates of insulin resistance. HOMA-IR or log (HOMA-IR) may not give appropriate results in subjects with severely impaired or absent β -cell function.

Quantitative insulin sensitivity check index

The quantitative insulin sensitivity check index (QUICKI) is an empirically derived mathematical transformation of fasting blood glucose and plasma insulin concentrations that provides a reliable, reproducible, and accurate index of insulin sensitivity with excellent positive predictive power [25,70,80,81]. It is simply a variation of the HOMA equation as it transforms the data by taking both the logarithm and the reciprocal of the glucose-insulin product. Since fasting insulin levels do not have a normal distribution, log transformation improves its linear correlation with SI_{Clamp} . In order to solve the problem that it is difficult to maintain euglycemia in diabetic patients with fasting hyperglycemia and impaired β -cell function, addition of log (fasting glucose) to log (fasting insulin) provides a reasonable correction.

$$\text{QUICKI} = 1 / [\log(\text{fasting insulin, } \mu\text{IU/mL}) + \log(\text{fasting glucose, mg/dL})]$$

QUICKI has a substantially better linear correlation with SI_{Clamp} than SI derived from the minimal model or HOMA-IR, especially in obese and diabetic subjects [25,70,81]. In addition,

QUICKI has the strongest positive predictive power for determining development of diabetes [82], and is most correlated with changes in SI_{Clamp} after therapeutic interventions [70]. QUICKI is a simple, inexpensive, and non-invasive surrogate index. Compared with other surrogate indexes of insulin resistance, QUICKI is the most thoroughly evaluated and validated.

McAuley index

McAuley index [83] is used for predicting insulin resistance in normoglycemic individuals. Statistically, regression analysis method was used to estimate the cut-off values and the importance of various parameter for insulin resistance such as fasting insulin, triglycerides, aspartate aminotransferase, basal metabolic rate (body mass index [BMI]), and waist circumference.

$$\text{McAuley index} = \exp [2.63 - 0.28 \ln(\text{insulin in } \mu\text{IU/L}) - 0.31 \ln(\text{triglycerides in mmol/L})]$$

Matsuda index

The composite whole-body insulin SI including both hepatic and peripheral tissue insulin sensitivity developed by Matsuda and DeFronzo from OGTT data [26].

$$\text{SI}_{\text{Matsuda}} = 10,000 / \sqrt{[(G_0 \times I_0) \times (G_{\text{mean}} \times I_{\text{mean}})]}$$

G_0 : Fasting plasma glucose concentration (mg/dL) taken from time 0 of the OGTT

I_0 : Fasting plasma insulin concentration ($\mu\text{IU/L}$) taken from time 0 of the OGTT

G_{mean} : Mean plasma glucose concentration during OGTT (mg/dL)

I_{mean} : Mean plasma insulin concentration during OGTT ($\mu\text{IU/L}$)

The square root is used to correct for nonlinear distribution of insulin, and 10,000 is a scaling factor in the equation.

Stumvoll index

Stumvoll and Gerich proposed use of demographic data such as age, sex, and BMI in addition to plasma glucose (mmol/L) and insulin (pmol/L) responses during the OGTT to predict insulin sensitivity and β -cell function [84].

$$\text{SI}_{\text{Stumvoll}} = 0.156 - 0.0000459 \times I_{120(\text{pmol/L})} - 0.000321 \times I_{0(\text{pmol/L})} - 0.00541 \times G_{120(\text{mmol/L})}$$

I_0 , plasma insulin concentration during fasting

I_{120} , plasma insulin concentration at 120 minutes

G_{120} , plasma glucose concentration at 120 minutes

Avignon index

Avignon et al. [85] developed three insulin sensitivity indices: SiM, Sib, and Si2h by computation of fasting and 2-hour glucose and insulin data during OGTT. It is useful for blending both the determination of glucose tolerance and an estimate of insulin sensitivity in a single and simple test.

$$Sib = 10^8 / (I_0(\mu\text{IU/L}) \times G_0(\text{mmol/L}) \times \text{VD})$$

$$Si2h = 10^8 / (I_{120}(\mu\text{IU/L}) \times G_{120}(\text{mmol/L}) \times \text{VD})$$

$$SiM = [(0.137 \times Sib) + Si2h] / 2$$

I_0 , plasma insulin concentration during fasting

I_{120} , plasma insulin concentration at 120 minutes

G_0 , plasma glucose concentration during fasting

G_{120} , plasma glucose concentration at 120 minutes

VD, glucose distribution volume (150 mL/kg body weight)

Gutt index, ISI (0,120)

ISI (0,120) was calculated using the plasma glucose and insulin concentration from fasting (0 minute) and 120-minute samples from the OGTT [86]. The index correlates well with direct estimates of insulin sensitivity obtained from the HEC study.

$$ISI(0, 120) = 75,000 + (G_0 - G_{120})(\text{mmol/L}) \times 0.19 \times \text{body weight}_{(\text{kg})} / 120 \times G_{\text{mean}(0, 120)}(\text{mmol/L}) \times \text{Log}(I_{\text{mean}(0, 120)})(\mu\text{IU/L})$$

G_0 , plasma glucose concentration during fasting during OGTT

G_{120} , plasma glucose concentration at 120 minutes during OGTT

G_{mean} , mean plasma glucose concentration during OGTT

I_{mean} , mean insulin concentration during OGTT

Table 2. Indices of insulin resistance

Method	Measurement of insulin resistance
Dynamic test-based	
Direct measure of insulin resistance	
Hyperinsulinemic euglycemic clamp	$SI_{\text{Clamp}} = M / (G \times \Delta I)$
Insulin suppression test	SSPG (steady-state plasma glucose)
Indirect measure of insulin resistance	
Minimal model analysis of FSIVGTT	Computational model S_i : fractional glucose disappearance per insulin concentration unit S_G : ability of glucose <i>per se</i> to promote its own disposal and inhibit HGP in the absence of an incremental insulin effect
OGTT or MTT based indices	
Matsuda index	$ISI_{\text{Matsuda}} = 10,000 / \sqrt{[(G_0 \times I_0) \times (G_{\text{mean}} \times I_{\text{mean}})]}$
Stumvoll index	$ISI_{\text{Stumvoll}} = 0.156 - 0.0000459 \times I_{120}(\text{pmol/L}) - 0.000321 \times I_0(\text{pmol/L}) - 0.00541 \times G_{120}(\text{mmol/L})$
Avignon index	$SiM = [(0.137 \times Sib) + Si2h] / 2$
Gutt index, ISI (0,120)	$ISI(0, 120) = 75,000 + (G_0 - G_{120})(\text{mmol/L}) \times 0.19 \times \text{body weight}(\text{kg}) / 120 \times G_{\text{mean}}(0, 120)(\text{mmol/L}) \times \text{Log}(I_{\text{mean}}(0, 120))(\mu\text{IU/L})$
Belfiore index	$\text{Belfiore index} = 2(G_S / G_N) \times (I_S / I_N) + 1$
Static test-based indices	
Simple surrogate markers	
1/fasting insulin	Reciprocal of fasting plasma insulin concentration, $\mu\text{IU/mL}$
Glucose/insulin ratio	Ratio of fasting plasma glucose (mg/dL) and insulin ($\mu\text{IU/mL}$) concentration
HOMA-IR	$\text{HOMA-IR} = [\text{fasting insulin}(\mu\text{IU/mL})] \times [\text{fasting glucose}(\text{mmol/L})] / 22.5$
QUICKI	$\text{QUICKI} = 1 / [\log \text{fasting insulin}(\mu\text{IU/mL}) + \log(\text{fasting glucose, mg/dL})]$
McAuley's index	$\text{McAuley's index} = \exp[2.63 - 0.28 \ln(I_0) - 0.31 \ln(\text{TAG}_0)]$

SI, insulin sensitivity index; M, glucose disposal rate; G, steady state blood glucose concentration; ΔI , difference between fasting and steady-state plasma insulin concentrations; FSIVGTT, frequently sampled intravenous glucose tolerance test; HGP, hepatic glucose production; OGTT, oral glucose tolerance test; MTT, meal tolerance test; ISI, insulin sensitivity index; G_{mean} , mean plasma glucose concentration during OGTT; I_{mean} , mean insulin concentration during OGTT; G_0 , plasma glucose concentration during fasting; G_{120} , plasma glucose concentration at 120 minutes; I_0 , plasma insulin concentration during fasting ($\mu\text{IU/L}$); I_{120} , plasma insulin concentration at 120 minutes; HOMA-IR, homeostatic model assessment of insulin resistance; QUICKI, quantitative insulin sensitivity check index; TAG_0 , fasting triglyceride concentration.

Belfiore index

The Belfiore index was calculated with the normal value for basal glucose and insulin concentrations, and for mean normal value for glucose and insulin areas during OGTT [87].

$$\text{Belfiore index} = 2(G_S/G_N) \times (I_S/I_N) + 1$$

S, subjects

N, normal reference values

G_S, G_N : plasma glucose concentrations expressed as fasting values or as areas obtained during a standard OGTT at 0 and 2 hours

I_S, I_N : plasma insulin concentrations expressed as fasting values or as areas obtained during a standard OGTT at 0 and 2 hours

The indices for measuring insulin sensitivity/resistance described so far are summarized in Table 2. Direct measures of insulin sensitivity based on HEC or IST mainly reflect insulin sensitivity of skeletal muscle. On the other hand, indirect measures of insulin sensitivity based on FSIVGTT or surrogate indices based on OGTT or MTT reflect hepatic and peripheral insulin resistance. Static test-based insulin resistance indices primarily reflect hepatic insulin sensitivity.

CONCLUSIONS

To date, various methods have been developed to measure pancreatic β -cell function and insulin resistance/sensitivity. Each of these tests has advantages and limitations. The most appropriate method should be selected in consideration of the purposes, methods, and the practical situation. The hyperglycemic clamp and HEC study are still the gold standard methods for β -cell function and insulin sensitivity respectively, but these are invasive and labor intensive. Thus, it is necessary to develop a non-invasive, inexpensive, and easy method that best reflects the physiology of glucose and insulin metabolism. A better understanding about the how to measure β -cell function and insulin resistance/sensitivity will help us understand the pathophysiology of DM and further develop the treatment strategy and new drugs.

CONFLICTS OF INTEREST

No potential conflict of interest relevant to this article was reported.

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